# Neuroimaging and mathematical modelling Lesson 3: Diffusion Tensor Imaging 

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## Diffusion



Kleenex


Newspaper

## White matter: macroscopic



## White matter: macroscopic



## White matter: microscopy



## White matter: microscopy



## DTI: reconstruction



AJNR 2007

## Diffusion tensor imaging (DTI)



SLF


## Diffusion of water in water



HBWL

## Water diffusion in brain white matter

Anisotropic diffusion: Dx Dy DZ ...: Diffusion tensor
Unequally restricted in space, preferred directions


## Water diffusion in biological tissue

Still isotropic but restricted: apparent diffusion coefficient : ADC


HBWL

## Stochastic Movements

$\oplus$ The type/size of molecule and surroundings affect ease of random movement
© Diffusion coefficient = ease of movement
$\otimes$ More time or higher Diff. coeff. $\rightarrow$ wider distribution


High D
© This was described by A. Einstein in 1905
Annalen der Physik 1905;17:549

$$
\underset{\text { Unit: }}{\mathrm{Dm}} \mathrm{~m}=\frac{\operatorname{Av} g\left(x^{2}\right)}{2 t}
$$

## Example

## $\underset{U n i t: \mathrm{mm}^{2} / \mathrm{s} 2 t}{D}=\frac{\operatorname{Avg}\left(x^{2}\right)}{}$

$\mathrm{D}=1.0 \times 10^{-3} \mathrm{~mm} 2 / \mathrm{s}$ diffusivity of water in the parenchyma Se $t=35 \mathrm{~ms}$

Then $\mathrm{x}=8$ micrometer which is the diameter of an axon.

## Apparent Diffusion Coefficient

 (ADC)© Areas with higher rate of diffusion are brighter
(2) Little contrast between gray and white matter

* DWI calculation of ADC, relative rate of diffusion, is useful clinically (e.g. stroke)
(2) Not of much use in research?



## Brain Infarction (stroke)



Magnetic resonance imaging in acute stroke. Left: Diffusionweighted MRI in acute ischemic stroke performed 35 minutes after symptom onset. Right: Apparent diffusion coefficient (ADC) map obtained from the same patient at the same time.

## ADC (Apparent Diffusion Coefficient)

non-linear fitting
using image pixel values


$$
S=S_{0} \exp (-b \cdot A D C)
$$

linear fitting using natural
log of image pixel values


## Diffusion Weighted Imaging (DWI) Sequence

© Uses an EPI pulse sequence with bi-polar gradients applied during the sequence
© First gradient disrupts the magnetic phases of all protons
(8) Second gradient restores the phases of all stationary protons
(8) The restoration of signal is incomplete for protons that have moved (diffused) during the elapsed time

## Basic DWI Calculation

© Additional parameter in DWI is the b -value which defines both how strong the bi-polar gradients are and their duration

* Areas where diffusion occurs most rapidly will exhibit a greater decrease in MR signal as the $b$-value increases
© Collect multiple images each with a different b-value
® Typically estimated with just 2 b-values


## Diffusion Tensor Imaging

\& DTI relates image intensities to the relative mobility of water molecules in tissue and the direction of the motion
(2) Motion of a water molecules is a random walk (Brownian motion)
(3) Areas with relatively high mean diffusion will appear dark on the Diffusion weighted MRI images

## Currect terminology is irnportant

## Anatomy



## MR Tractography



## Streamlines

Trajectories

## Diffusion TENSOR imaging (DTI)



## Diffusion Tensor Imaging (DTI)



## Diffusion Tensor Imaging (DTI)

$\circledast$ Mobility in a given direction is described by ADC
© The tissue diffusivity is described by the tensor D
(1) The diffusion equation

$$
\text { Attenuation }=\frac{A(b)}{A(0)}=\exp \left(-b \sum_{i, j=1,2,3} x_{i j} \cdot D_{i j}\right)=\exp (-b \cdot A D C)
$$


(1) Diffusion is represented by a $3 \times 3$ tensor*

${ }^{*}$ P. Basser and D. Jone, NMR in Biomedicine, 2002.

## Diffusion Tensor

$$
\mathrm{D}=\left[\begin{array}{lll}
D_{x x} & D_{x y} & D_{x z} \\
D_{x y} & D_{y y} & D_{y z} \\
D_{x z} & D_{y z} & D_{z z}
\end{array}\right]
$$

(2) Diffusion properties described with a 3 X 3 symmetric tensor matrix

* Diagonal elements of $\mathbf{D}(D x x, D y y, D z z)$ are the ADC values along $x, y$ and $z$ axes respectively
(2) Off-diagonal elements ( $D x y, D x z, D y z$ ) represent the correlation between molecular displacements in orthogonal directions


## Diffusion Tensor Imaging (DTI)

© Brain Tissue types
® Cerebrospinal fluid (CSF)
© Gray matter (GM)
$\oplus$ White matter (WM)
$\circledast$ Mixing of tissues


## Diffusion Tensor Imaging (DTI)

© Invariant Anisotropy Indices $\oplus$ Fractional Anisotropy (FA)*
© Relative Anisotropy (RA)*
® Volume Ratio (VR)*

"D. LeBihan, NMR Biomedicine., 2002.

## DTI Calculation

$\otimes$ Eigenvalues of the diffusion tensor $\left(\lambda_{x}, \lambda_{y}\right.$, and $\left.\lambda_{z}\right)$ provides length of the ellipsoid in the three principal directions of diffusivity
$\otimes$ Eigenvectors provide information about the direction of diffusion
$\oplus$ The eigenvector corresponding to the largest eigenvalue is used as the main direction of diffusion

* Maps are constructed of various measures of anisotropy from the eigenvalues and eigenvectors


## Isotropic diffusion



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## Anisotropic diffusion



## Apparent Difussion Coefficient (ADC)

Multicompartment system in vivo
Intra cellular volume $=70 \%$
Extra cellular volume $=20 \%$
Vascular volume $=10 \%$
Membranes, mitochondria ect.

$$
\begin{gathered}
\mathbf{D}_{\mathbf{I C V}}<\mathbf{D}_{\mathbf{E C V}} \\
\mathrm{ADC}=0.7-1.2 \cdot 10^{-9} \mathrm{~m}^{2} / \mathrm{s} \\
\mathrm{D}_{\mathrm{H}_{2} \mathrm{O}}=3 \cdot 10^{-9} \mathrm{~m}^{2} / \mathrm{s}
\end{gathered}
$$


$\mathrm{T}=37^{\circ} \mathrm{C}$

Restricted diffusion
Dependence of diffusion time
Dependence of dirrections : Isotropic > < Anisotropic diffusion


HBWL


